





Simulated Excitation Patterns in the Atria and Their Corresponding Electrograms

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- Introduction: Our aim and what's new, relation to MICROCARD
- **Methods:** Model, EGM calculation
- **Results:** Excitation patterns and their EGMs
- Discussion: What could be reproduced and what not?
- **Outlook:** What will future studies have to consider?

Introduction I: What is our aim and what's new?



- Electroanatomical mapping (EAM) is a crucial method to understand rhythm disturbances and to tackle them (e.g. for ablation therapy)
- Excitation dynamics may be characterised using electrograms (EGMs)
- In silico models provide a way to simulate different patterns and to study them systematically
- Such insights may help to **enhance clinical EAM systems** (set up and verification)

Introduction II: What is our aim and what's new?

- So far, patterns observed only in simple 2- or 3D patches or geometries not considering e.g. differing wall thickness
- We consider varying electrical properties and a realistic volumetric geometry
- Characterisation: Place electrodes above abnormal excitation patterns and compare changes in EGM amplitude and morphology to the healthy case
- Baseline to MICROCARD project









 $y \ (mm)$

Methods I

- Volumetric right atrial model from MRI patient data
- 2.3 mio. tetrahedra with an avg. edge length of ~ 0.6 mm
- Applied different electric properties, depending on the atrial region
- Simulations: openCARP [1], visualisation: Meshalyzer [2]
- Ionic model: Courtemanche-Ramirez-Nattel [3]
- [1] Plank* et al., Comp. Meth. Prog. in Biomed. (2021)
- [2] E. Vigmond et al., doi:10.35097/881 (2023)
- [3] Courtemanche et al., Am. Journal of Phys. (1998)







Methods II

Place 4 x 4 multielectrode array above excitation patterns to calculate uni- and bipolar EGMs



uEGMs calculated via the **infinite volume conductor method**:

 $\phi_{\mathbf{e}} = \frac{1}{4\pi\sigma_{\mathbf{b}}} \int_{V} \frac{\sigma_{\mathbf{i}} \cdot \vec{\nabla} V_{\mathbf{m}}}{||\vec{x} - \vec{x}_{\mathbf{src}}||} \mathrm{d}V \quad \overset{\sigma_{\mathbf{b}},\sigma_{\mathbf{i}}: \text{ bath & intracell. conductivity}}{||\vec{x} - \vec{x}_{\mathbf{src}}||: \text{ electrode - source distance}}$

biEGMs calculated as the difference between two neighbouring uEGMs

[4] Taken from https://www.cardiovascular.abbott/de/de/hcp/electrophysiology/advisor-hd-grid.html (last access 3rd July 2023)





Results: SIN Case





- Sinus rhythm: No abnormal excitation pattern
- EGMs: reference for the healthy case

- Fast activation along pectinate muscles, approx. plane wave propagation
- uEGMs (above): biphasic and almost symmetric



biEGM (right): triphasic with pronounced minimum

Results: Line of Block (LOB) Case





 Propagating wave collides with a nonconducting region ()

- uEGMs (above): Double potentials, lowered amplitude
- biEGM (right): Multiple deflections



C4

B4

50



Results: Slow Conduction Zone (SCZ) Case





- Wave collides with a slowly-conducting
 - region (), still allowing for excitation

propagation

• uEGMs (above): Small deflections, severe reduction in amplitude

biEGM (right): Triphasic, non-symmetric



Results: Pivoting (PIV) Wave Case





Wave needs to circumvent a non-

conducting block



biEGM (right): Triphasic, non-symmetric



Results: Propagation Through GAP Case





 Wave propagating through a conducting gap in a LOB

uEGMs (above): Double potentials after the LOB, reduced amplitudes

biEGM (right): Triphasic, almost symmetric





Results: Two Colliding (COL) Waves Case



Two wave fronts colliding (SIN wave with ectopic beat from right pulmonary vein)

- uEGMs (above): Almost single-phasic
- biEGM (right): biphasic with pronounced R-peak



Discussion and Conclusion



Could reproduce important features of clinical EGMs for all patterns (e.g. double potentials in uEGMs for the LOB or multiple deflections in the SCZ case found in EAM)

However, fractionation not properly reproduced as well as e.g. narrowly spaced biEGMs for the PIV case

In principle capable of correctly simulating EGM properties but not with all desired details requires follow-up studies

Outlook: Improvements in Further Studies



Finer (subcellular) mesh resolution using the EMI model [5] contribution to MICROCARD

More properly reproduce characteristics of e.g. non-conducting blocks (intermediate zones that decelerate the wave before it collides with the block)

More sophisticated EGM calculation approaches [6]

Considering spatial extension of the electrode [7]

- [5] Tveito et al., Springer Briefs on Computing (2020)
- [6] Bishop et al., IEEE Trans. on Biomed. Eng. (2011)
- [7] Nairn et al., Comp. in Cardiol. (2020)



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